



(19)

Europäisches Patentamt

European Patent Office

Office européen des brevets



(11)

EP 0 812 187 B1

(12)

EUROPEAN PATENT SPECIFICATION

(45) Date of publication and mention of the grant of the patent:
02.05.2003, Bulletin 2003/18

(51) Int Cl.7: **A61K 9/16**

(21) Application number: 96904612.7

(86) International application number:
PCT/US96/01845

(22) Date of filing: 09.02.1996

(87) International publication number:
WO 96/025150 (22.08.1996 Gazette 1996/38)

(54) SOLID NANOPARTICULATE PHARMACEUTICAL COMPOSITION

FESTE PHARMAZEUTISCHE ZUSAMMENSETZUNG AUS NANOPARTIKELN

COMPOSITION SOLIDE DE NANOPARTICULES PHARMACEUTIQUES

(84) Designated Contracting States:
AT BE CH DE DK ES FR GB GR IE IT LI LU MC NL
PT SE

(72) Inventors:

- DESIENO, Mark, A.
Gilbertsville, PA 19525 (US)
- STETSKO, Gregg
San Diego, CA 92121 (US)

(30) Priority: 13.02.1995 US 387651

(74) Representative: Dörries, Hans Ulrich, Dr. et al
Dörries, Frank-Molnia & Pohlman,
Triftstrasse 13
80538 München (DE)

17.12.1997 Bulletin 1997/51

(56) References cited:
EP-A- 0 164 967

(73) Proprietor: Elan Pharma International Limited
Shannon, Co. Clare (IE)

EP-A- 0 514 967

EP 0812187 B1

Note: Within nine months from the publication of the mention of the grant of the European patent, any person may give notice to the European Patent Office of opposition to the European patent granted. Notice of opposition shall be filed in a written reasoned statement. It shall not be deemed to have been filed until the opposition fee has been paid. (Art. 99(1) European Patent Convention).

Description**Field Of The Invention**

5 [0001] This invention relates to nanoparticulate drug particles and pharmaceutical compositions containing them. The invention further relates to the use of and compositions as medicaments.

Background of Invention

10 [0002] Bioavailability is the degree to which a drug becomes available to the target tissue after administration. Many factors can affect bioavailability including the dosage form and various properties, e.g., dissolution rate of the drug. Poor bioavailability is a significant problem encountered in the development of pharmaceutical compositions, particularly those containing an active ingredient that is poorly soluble in water. Poorly water soluble drugs, i.e., those having a solubility less than about 10 mg/ml, tend to be eliminated from the gastrointestinal tract before being absorbed into 15 the circulation. Moreover, poorly water soluble drugs tend to be unsafe for intravenous administration techniques, which are used primarily in conjunction with fully soluble drug substances.

[0003] It is known that the rate of dissolution of a particulate drug can increase with increasing surface area, i.e., decreasing particle size. Consequently, methods of making finely divided drugs have been studied and efforts have been made to control the size and size range of drug particles in pharmaceutical compositions. For example, dry milling 20 techniques have been used to reduce particle size and hence influence drug absorption. However, in conventional dry milling, as discussed by Lachman, et al., *The Theory and Practice of Industrial Pharmacy*, Chapter 2, "Milling", p. 45 (1986), the limit of fineness is reached in the region of 100 microns (100,000 nm) when material cakes on the milling chamber. Lachman, et al. note that wet grinding is beneficial in further reducing particle size, but that flocculation restricts the lower particle size limit to approximately 10 microns (10,000 nm). However, there tends to be a bias in the 25 pharmaceutical art against wet milling due to concerns associated with contamination. Commercial airjet milling techniques have provided particles ranging in average particle size from as low as about 1 to 50 μm (1,000-50,000 nm).

[0004] U.S. Patent No. 5,145,684 discloses particles of a drug substance having a surface modifier absorbed on the 30 surface thereof and methods for the preparation thereof by wet grinding. These particles have demonstrated significant pharmaceutical utility. Suitable surface modifiers described include various polymers. The surface modifiers disclosed include Pluronic F68 and F108, which are block copolymers of ethylene oxide and propylene oxide, Tetronic 908, which is a tetrafunctional block copolymer derived from sequential addition of propylene oxide and ethylene oxide to ethylene diamine; sodium dodecylsulfate, dialkyl esters of sodium sulfosuccinic acid such as Aerosol OTTM, sodium lauryl sulfate, and TritonTM X-200. Pluronic and Tetronic are trademarks of BASF. This patent notes the difficulty of forming nanoparticulate drug containing compositions which have good bioavailability and also are generally impervious to increase in 35 size due to agglomeration of drug particles.

[0005] EP-A2-0 164 967 provides a pharmaceutical composition comprising a plurality of beads comprising solid steroid particles which are bound onto a particulate core by a water-soluble binder.

[0006] EP-A1-0 514 967 relates to sugar or starch beads coated with a composition consisting of a low-solubility 40 drug and of a cellulose derivative, a polyethylene glycol or derivative thereof and a waxy copolymer solid and a process for preparing such beads.

[0007] It is desirable to provide a pharmaceutical composition containing a nanoparticulate drug which can be stored for periods of time without undue loss of bioavailability due to agglomeration into larger size particles.

Summary of the Invention

45 [0008] We have discovered that nanoparticulate drug particles which can be coated on to a carrier particle to be formulated into pharmaceutical compositions exhibiting high bioavailability.

[0009] More specifically, in accordance with this invention, there are provided pharmaceutical compositions comprising nanoparticles of a low solubility drug associated with a steric stabilizer and a film dispersing agent wherein 50 dissolution of the film results in substantial redispersion of the drug nanoparticles.

[0010] In particular, in accordance with the invention, there is provided a solid nanoparticulate pharmaceutical composition comprising:

55 (a) a solid carrier composition, and coated onto the solid carrier composition
 (b) a nanoparticulate drug matrix composition comprising:

(1) a nanoparticulate crystalline drug having a solubility in water of less than 10 mg/ml;
 (2) 0.1% to 90%, based on the weight of the drug, of a hydrophilic or amphophilic steric stabilizer associated

with the surface of the nanoparticulate drug; and
 (3) 0.05% to 50%, based on the weight of the drug, of a water-soluble film dispersing agent associated with the surface of the drug,

5 wherein dissolution of the solid carrier composition results in substantial redispersion of the nanoparticulate drug particles.

[0011] This invention also provides a stable pharmaceutical composition comprising a carrier particle having on its surface a film comprising nanoparticles of a low solubility drug associated with a steric stabilizer and a film dispersing agent, wherein dissolution of the film results in substantial redispersion of the drug nanoparticles.

10 [0012] In a particularly valuable and important embodiment of the invention there is provided a pharmaceutical composition comprising a carrier particle having on its surface a film comprising nanoparticles of a low solubility drug associated with a steric stabilizer and a film dispersing agent, wherein dissolution of the film results in substantial redispersion of the drug nanoparticles and an overcoat applied over said film comprising polyvinylpyrrolidone/polyethylene glycol (PVP/PEG).

15 [0013] The pharmaceutical compositions of this invention are useful as medicaments with a variety of drugs.

[0014] It is a particularly advantageous feature of this invention that the pharmaceutical compositions described herein exhibit high bioavailability.

[0015] Still another advantageous feature of this invention is that the compositions are stable against agglomeration of the drug nanoparticles into larger sizes because the compositions are readily redispersible.

20 [0016] Other advantageous features will become readily apparent upon reference to the following Description of Preferred Embodiments.

Description of Preferred Embodiments

25 [0017] This invention is based partly on the discovery that drug particles having an extremely small effective average particle size can be prepared by wet milling in the presence of grinding media in conjunction with a surface modifier, and that such particles are stable and do not appreciably flocculate or agglomerate due to interparticle attractive forces and can be formulated into pharmaceutical compositions exhibiting unexpectedly high bioavailability. While the invention is described herein primarily in connection with its preferred utility, i.e., with respect to nanoparticulate drug substances for use in pharmaceutical compositions, it is also believed to be useful in other applications such as the preparation of particulate dispersions for use in image and magnetic recording elements.

[0018] The particles of this invention comprise a drug substance. The drug substance exists as a discrete, crystalline phase. The crystalline phase differs from a noncrystalline or amorphous phase which results from precipitation techniques, such as described in EPO 275,796 cited above.

35 [0019] The invention can be practiced with a wide variety of drug substances. The drug substance preferably is present in an essentially pure form. The drug substance must be poorly soluble and dispersible in at least one liquid medium. By "poorly soluble" it is meant that the drug substance has a solubility in water of less than about 10 mg/ml and preferably less than about 1 part in greater than 1,000,000 parts of water. A preferred liquid dispersion medium is water. However, the invention can be practiced with other liquid media in which a drug substance is poorly soluble and dispersible including, for example, aqueous salt solutions, safflower oil and solvents such as ethanol, t-butanol, hexane and glycol. The pH of the aqueous dispersion media can be adjusted by techniques known in the art.

40 [0020] Suitable drug substances can be selected from a variety of known classes of drugs including, for example, analgesics, anti-inflammatory agents, anthelmintics, anti-arrhythmic agents, antibiotics (including penicillins), anticoagulants, antidepressants, antidiabetic agents, antiepileptics, antihistamines, antihypertensive agents, antimuscarinic agents, antimycobacterial agents, antineoplastic agents, immunosuppressants, antithyroid agents, antiviral agents, anxiolytic sedatives (hypnotics and neuroleptics), astringents, beta-adrenoceptor blocking agents, blood products and substitutes, cardiac inotropic agents, contrast media, corticosteroids, cough suppressants (expectorants and mucolytics), diagnostic agents, diagnostic imaging agents, diuretics, dopaminergics (antiparkinsonian agents), haemostatics, immunological agents, lipid regulating agents, muscle relaxants, parasympathomimetics, parathyroid calcitonin and biphosphonates, prostaglandins, radio-pharmaceuticals, sex hormones (including steroids), anti-allergic agents, stimulants and anoretics, sympathomimetics, thyroid agents, vasodilators and xanthines. Preferred drug substances include those intended for oral administration and intravenous administration. A description of these classes of drugs and a listing of species within each class can be found in Martindale, The Extra Pharmacopoeia, Twenty-ninth Edition, The Pharmaceutical Press, London, 1989, the disclosure of which is hereby incorporated by reference in its entirety.

50 [0021] The drug substances are commercially available and/or can be prepared by techniques known in the art.

[0022] Preferred and representative illustrative species of drug substances useful in the practice of this invention include danazol, naproxen and cylosporin.

55 [0023] The matrix of this invention comprises a steric stabilizer. The steric stabilizer is a hydrophilic or amphophilic

compound having steric stabilizing properties such as a physical or chemical anchored molecule with backbone and side chains which import a physical barrier to interaction of the small particles. Examples of steric stabilizers can be found in Lieberman, Rieger, Bunker *Pharmaceutical Dosage Forms: Disperse Systems*, Volume 1.

5 [0023] Preferred steric stabilizers are gelatin, casein, lecithin, gum acacia, cholesterol, tragacanth, sorbitan esters, polyoxyethylene alkyl esters, polyoxyethylene caster oil derivatives, polyoxyethylene, sorbitan fatty acid esters, polyethyleneglycols, polyoxyethylene stearates, carboxymethylcellulose calcium, carboxymethylcellulose sodium, methylcellulose, hydroxyethylcellulose, hydroxypropylcellulose, hydroxypropylmethylcellulose, phthalate, non crystalline cellulose, polyvinyl alcohol and polyvinylpyrrolidone.

10 [0024] d-Alpha tocopheryl polyethylene glycol 1000 succinate is described by the manufacturer (Eastman Chemical Products, Inc., a division of Eastman Kodak Company, Kingsport, Tennessee 37622) in a product brochure dated February 4, 1983 as "prepared from crystalline d-Alpha Tocopheryl Acid Succinate NF by esterification of the acid group with polyethylene glycol 1000", as also being named "Vitamin E TPGS", as being a "[p]ale yellow, waxy solid" having a specific gravity at 45°C. of approximately 1.06 and a melting point of approximately 40°C., and in the opinion of the manufacturer as being "recognized as safe ("GRAS") when used as an oral dietary supplement of vitamin E."

15 [0025] The preferred amount of each of the cellulose derivative, polyethylene glycol or derivative thereof and waxy solid in the first composition of matter aspect of the invention is from about 5% to about 30% by weight of the coating composition.

20 [0026] The preferred amount of each of the hydropropyl methylcellulose, polyethylene glycol and polyoxyethylene-polyoxypropylene-polyoxyethylene block copolymer in the preferred first composition of matter aspect of the invention is from about 5% to about 15% by weight of the coating composition.

25 [0027] The most preferred steric stabilizer is polyvinylpyrrolidone.

[0028] The film matrix also comprises a film dispersing agent. The film dispersing agent is a water soluble compound associated with the surface of the nanoparticle. Film dispersing agents are those materials which oppose the binding capability of the film when placed in an aqueous environment enhancing film solubility or by swelling and disrupting films.

30 [0029] Preferred film dispersing agents are mannitol, sodium lauryl sulfate, mono and disaccharides. Sodium lauryl sulfate is particularly preferred. Sodium lauryl sulfate is also named as "[s]ulfuric acid monododecyl ester sodium salt; sodium starch glycolate; croscarmellose sodium" and "[s]odium monododecyl sulfate" and is described as ...a mixture of sodium alkyl sulfates consisting chiefly of sodium lauryl sulfate $[CH_3(CH_2)_{10}CH_2OSO_3Na]$. The combined content of sodium chloride and sodium sulfate is not more than 8.0 percent.

35 [0030] In the dissolution step of the process aspect of the invention the temperature of warming can be in the range from room temperature to about 100°C. and is preferably in the range from 50°C. to 60°C. About 80% of the total amount of water needed is used for the dissolution and suspension steps and the remainder is used for rinsing the last amounts of solution and suspension from the equipment. Preferably the polyethylene glycol or derivative thereof and the waxy solid are dissolved first, and the cellulose derivative is then added and dissolved. The low solubility drug is added to the resulting solution with agitation to form a suspension. The dissolution and suspension steps are carried out with conventional mixing equipment. The suspension is preferably passed through a colloid mill before carrying out the coating step and agitation is maintained during the coating step. The coating and drying steps are preferably carried out in a fluid bed processor with inlet air temperature in the range from 50°C. to 70°C. with preheating of the sugar or sugar/starch beads. After drying the coated beads are sifted to produce coated beads of the desired particle size, preferably 16-60 mesh.

40 [0031] Preferred film matrices comprise nanoparticles of a low solubility drug having about 0.1% to about 60% of a steric stabilizer and about 0.05 to about 50% of a film dispersing agent, based on the weight of the low solubility drug, associated with the nanoparticle surface.

45 [0032] In a particularly preferred embodiment of this invention, the film matrix is overcoated with polyvinylpyrrolidone (PVP)/polyethylene glycol (PEG). This overcoat provides improved stability to the pharmaceutical composition.

50 [0033] The overcoating is prepared by casting PVP such as Providone with different types and units of PEG such as PEG 600, PEG 1000 and PEG 1450 and mixtures thereof. Polyethylene glycol is described as "an addition polymer of ethylene oxide and water, represented by the formula $H(OCH_2CH_2)_nOH$ in which n represents the average number of oxyethylene groups." The variants are designated by "nominal value" of "average molecular weight", which is explained as follows:

55 [0034] The average molecular weight is not less than 95.0 percent and not more than 105.0 percent of the labeled nominal value if the labeled nominal value is below 1000; it is not less than 90.0 percent and not more than 110.0 percent of the labeled nominal value if the labeled nominal value is between 1000 and 7000; it is not less than 87.5 percent and not more than 112.5 percent of the labeled nominal value if the labeled nominal value is about 7000.

[0035] Polyethylene glycols having nominal average molecular weights in the range from 300 to 8000 are described. Polyethylene glycol 3350 is the preferred polyethylene glycol of the invention.

[0036] Providone, USP is the USAN name for 2-Pyrrolidinone, 1-ethenyl-homopolymer of 1-vinyl-2-pyrrolidinone polymer. It is sold under the trademarks KOLIDON (BASF), PLASDONE (International Specialty Products) and VINISIL

(Abbott).

[0037] The weight ratio of PEG/PVP is generally from 1 to about 5. The pharmaceutical film matrix is formed by dissolving the PEG and PVP in a suitable solvent.

[0038] Suitable carriers comprise sugar spheres, maltodextrin, microcrystalline cellulose, microcrystal cellulose/sodium carboxymethylcellulose, granular dextrose, dicalcium phosphate, tricalcium phosphate, mono and discaccardes. The preferred carriers are sugar spheres. Sugar Spheres are described as containing "not less than 62.5 percent and not more than 91.5 percent of sucrose ($C_{12}H_{22}O_{11}$), calculated on the dried basis, the remainder consisting chiefly of starch" and as consisting of "approximately spherical particles of a labeled nominal size range" and correspond to the sugar or sugar/starch beads of the invention. They can also be or be referred to as granules, particles, pellets or nonpareils and are from about 2 millimeters or about 10 mesh to about 0.2 millimeter or about 80 mesh, preferably from about 20 mesh to about 70 mesh, in diameter or longest dimension before coating. After coating the preferred diameter or longest dimension is from about 16 mesh to about 60 mesh.

[0039] The overcoat can be coated over the film by spraying the solution onto the substrate by using a vented pan or fluid bed coating unit with inlet air temperature of between 40-80°C.

[0040] The dispersion of surface modified nanoparticles can be spray coated onto sugar spheres or onto a pharmaceutical excipient in a fluidized bed.

[0041] The spray coating is accomplished by techniques well known in the art. Sugar spheres are described as containing "not less than 62.5 percent and not more than 91.5 percent of surose ($C_{12}H_{22}O_{11}$), calculated on the dried basis, the remainder consisting chiefly of starch" and as consisting of "approximately spherical particles of a labeled nominal size range" and correspond to the sugar or sugar/starch beads of the invention. They can also be or be referred to as granules, particles, pellets or nonpareils and are from about 2 millimeters or about 10 mesh to about 0.2 millimeter or about 80 mesh, preferably from about 20 mesh to about 70 mesh, in diameter or longest dimension before coating. After coating the preferred diameter or longest dimension is from about 16 mesh to about 60 mesh.

[0042] The composition can be formed into a capsule shell. The capsule shell of this composition of matter can be any pharmaceutically acceptable capsule shell but is preferably a gelatin capsule shell and can be a soft gelatin capsule shell or a hard gelatin capsule shell but is preferably a hard gelatin capsule shell and is of suitable size for containing from about 0.5 milligram to about 700 milligrams of the composition of matter. Conventional machinery and technique are used in filling the capsule shells.

[0043] The particles of this invention can be prepared in a method comprising the steps of dispersing a drug substance in a liquid dispersion medium and applying mechanical means in the presence of grinding media to reduce the particle size of the drug substance to an effective average particle size of less than about 400 nm. The particles can be reduced in size in the presence of a surface modifier. Alternatively, the particles can be contacted with a surface modifier after attrition.

[0044] A general procedure for preparing the particles of this invention is set forth below. The drug substance selected is obtained commercially and/or prepared by techniques known in the art in a conventional coarse form. It is preferred, but not essential, that the particle size of the coarse drug substance selected be less than about 100 μm as determined by sieve analysis. If the coarse particle size of the drug substance is greater than about 100 μm , then the particles of the drug substance be reduced in size to less than 100 μm using a conventional milling method such as airjet or fragmentation milling.

[0045] The coarse drug substance selected can then be added to a liquid medium in which it is essentially insoluble to form a premix. The concentration of the drug substance in the liquid medium can vary from about 0.1-60%, and preferably is from 5-30%(w/w). It is preferred, but not essential, that the surface modifier be present in the premix. The concentration of the surface modifier can vary from about 0.1 to about 90%, and preferably is 1-75%, more preferably 20-60%, by weight based on the total combined weight of the drug substance and surface modifier. The apparent viscosity of the premix suspension is preferably less than about 1000 centipoise.

[0046] The premix can be used directly by subjecting it to mechanical means to reduce the average particle size in the dispersion to less than 400 nm. It is preferred that the premix be used directly when a ball mill is used for attrition. Alternatively, the drug substance and, optionally, the surface modifier, can be dispersed in the liquid medium using suitable agitation, e.g., a roller mill or a Cowles type mixer, until a homogeneous dispersion is observed in which there are no large agglomerates visible to the naked eye. It is preferred that the premix be subjected to such a premilling dispersion step when a recirculating media mill is used for attrition.

[0047] The mechanical means applied to reduce the particle size of the drug substance conveniently can take the form of a dispersion mill. Suitable dispersion mills include a ball mill, an attritor mill, a vibratory mill, and media mills such as a sand mill and a bead mill. A media mill is preferred due to the relatively shorter milling time required to provide the intended result, i.e., the desired reduction in particle size. For media milling, the apparent viscosity of the premix preferably is from about 100 to about 1000 centipoise. For ball milling, the apparent viscosity of the premix preferably is from about 1 up to about 100 centipoise. Such ranges tend to afford an optimal balance between efficient particle fragmentation and media erosion.

[0048] The grinding media for the particle size reduction step can be selected from rigid media preferably spherical or particulate in form having an average size less than about 3 mm and, more preferably, less than about 1 mm. Such media desirably can provide the particles of the invention with shorter processing times and impart less wear to the milling equipment. The selection of material for the grinding media is not believed to be critical. We have found that 5 zirconium oxide, such as 95% ZrO stabilized with magnesia, zirconium silicate, and glass grinding media provide particles having levels of contamination which are believed to be acceptable for the preparation of pharmaceutical compositions. However, other media, such as stainless steel, titania, alumina, and 95% ZrO stabilized with yttrium, are expected to be useful. Preferred media have a density greater than about 3 g/cm³.

[0049] The attrition time can vary widely and depends primarily upon the particular mechanical means and processing 10 conditions selected. For ball mills, processing times of up to five days or longer may be required. On the other hand, processing times of less than 1 day (residence times of one minute up to several hours) have provided the desired results using a high shear media mill.

[0050] The particles must be reduced in size at a temperature which does not significantly degrade the drug substance. Processing temperatures of less than about 30°C-40°C. are ordinarily preferred. If desired, the processing 15 equipment can be cooled with conventional cooling equipment. The method is conveniently carried out under conditions of ambient temperature and at processing pressures which are safe and effective for the milling process. For example, ambient processing pressures are typical of ball mills, attritor mills and vibratory mills. Processing pressures up to about 20 psi (1.4 kg/cm²) are typical of media milling.

[0051] The surface modifier, if it was not present in the premix, must be added to the dispersion after attrition in an 20 amount as described for the premix above. Thereafter, the dispersion can be mixed, e.g., by shaking vigorously. Optionally, the dispersion can be subjected to a sonication step, e.g., using an ultrasonic power supply. For example, the dispersion can be subjected to ultrasonic energy having a frequency of 20-80 kHz for a time of about 1 to 120 seconds.

[0052] The relative amount of drug substance and surface modifier can vary widely and the optimal amount of the 25 surface modifier can depend, for example, upon the particular drug substance and surface modifier selected, the critical micelle concentration of the surface modifier if it forms micelles, etc. The surface modifier preferably is present in an amount of about 0.1-10 mg per square meter surface area of the drug substance. The surface modifier can be present in an amount of 0.1-90%, preferably 20-60% by weight based on the total weight of the dry particle.

[0053] As indicated by the following examples, not every combination of surface modifier and drug substance provides 30 the desired results. Consequently, the applicants have developed a simple screening process whereby compatible surface modifiers and drug substances can be selected which provide stable dispersions of the desired particles. First, coarse particles of a selected drug substance of interest are dispersed in a liquid in which the drug is essentially insoluble, e.g., water at 5%(w/w) and milled for 60 minutes in a DYNOMILL under the standard milling conditions which are set forth in Example 1 which follows. The milled material is then divided into aliquots and surface modifiers are added at concentrations of 2, 10 and 50% by weight based on the total combined weight of the drug substance 35 and surface modifier. The dispersions are then sonicated (1 minutes, 20 kHz) to disperse agglomerates and subjected to particle size analysis by examination under an optical microscope (1000 x magnification). If a stable dispersion is observed, then the process for preparing the particular drug substance surface modifier combination can be optimized in accordance with the teachings above. By stable it is meant that the dispersion exhibits no flocculation or particle agglomeration visible to the naked eye at least 15 minutes, and preferably, at least two days or longer after preparation.

[0054] The resulting dispersion of this invention is stable and consists of the liquid dispersion medium and the above-described particles. The dispersion of surface modified drug nanoparticles can be spray coated onto sugar spheres or onto a pharmaceutically excipient in a fluidbed spray coater by techniques well known in the art. 40

[0055] Pharmaceutical compositions according to this invention include the particles described above and a pharmaceutically acceptable carrier thereof. Suitable pharmaceutically acceptable carriers are well known to those skilled 45 in the art. These include non-toxic physiologically acceptable carriers, adjuvants or vehicles for parenteral injection, for oral administration in solid or liquid form, for rectal administration, and the like. A method of treating a mammal in accordance with this invention comprises the step of administering to the mammal in need of treatment an effective amount of the above-described pharmaceutical composition. The selected dosage level of the drug substance for treatment is effective to obtain a desired therapeutic response for a particular composition and method of administration.

50 The selected dosage level therefore, depends upon the particular drug substance, the desired therapeutic effect, on the route of administration, on the desired duration of treatment and other factors. As noted, it is a particularly advantageous feature that the pharmaceutical compositions of this invention exhibit unexpectedly high bioavailability as illustrated in the examples which follow. Furthermore, it is contemplated that the drug particles of this invention provide more rapid onset of drug action and decreased gastrointestinal irritancy.

[0056] It is contemplated that the pharmaceutical compositions of this invention will be particularly useful in oral and 55 parenteral, including intravenous, administration applications. It is expected that poorly water soluble drug substances, which prior to this invention, could not have been administered intravenously, may be administered safely in accordance with this invention. Additionally, drug substances which could not have been administered orally due to poor bioavail-

ability may be effectively administered in accordance with this invention.

[0057] The following composition in accordance with the first composition of matter aspect of the invention was prepared using the process aspect of the invention.

5 Example 1

[0058]

	Ingredient	Amount (kg.)
10	(5 α ,17 α)-1'-(Methylsulfonyl)-1'H-pregn-20-yno[3,2-c]pyrazol-17-ol	0.720
	Poloxamer 188, NF	0.0900
	Polyethylene Glycol 3350, NF	0.144
15	Hydroxypropyl Methylcellulose, USP	0.100
	Sugar Spheres (30,35 mesh), NF	0.450
	Purified Water, USP (removed during processing)	2.46
	Total amount of dry ingredients	1.500

20 A portion of this composition sufficient to provide 200 mg. of the steroid drug when filled into a hard gelatin capsule has the following composition:

	Ingredient	Mg./Capsule
25	(5 α ,17 α)-1'-(Methylsulfonyl)-1'H-pregn-20-yno[3,2-c]pyrazol-17-ol	200.
	Poloxamer 188, NF	25.0
	Polyethylene Glycol 3350, NF	40.0
30	Hydroxypropyl Methylcellulose, USP	27.8
	Sugar Spheres (30,35 mesh), NF	125.
	Total Capsule Fill Weight	418.

35 [0059] The amount of drug in each capsule can be varied by varying the capsule fill weight, the amount of drug in the coating composition or the amount of coating composition coated onto the sugar or sugar/starch beads.

[0060] The composition of Example 1 was shown to have improved bioavailability over a conventional tablet composition of the same drug when compared in the dog. The following conventional tablet composition was prepared using a conventional table preparation method.

40 Comparative Example

[0061]

	Ingredient	Mg./Tablet
45	(5 α ,17 α)-1'-(Methylsulfonyl)-1'H-pregn-20-yno[3,2-c]pyrazol-17-ol	50.0
	Microcrystalline Cellulose, NF (Avicel pH 101)	60.0
	Poloxamer 188, NF	6.0
50	Lactose, NF (Spray Dry)	161.5
	Croscarmellose Sodium, FN (Ac-Di-Sol)	15.0
	Magnesium, Stearate, NF	1.5
	Providone, USP (PVP, K29-32)	6.0
	Total	300.0

55

Example 2 - Preparation of a Pharmaceutical Composition

[0062] Two danazol dispersions were prepared by dissolving the PVP in water, dispersing the danazol substance, and milling by use of an agitating bead mill. The dispersion was milled to a final mean particle size of between 150-250 nm.

[0063] The pharmaceutical compositions were prepared by spray coating onto 5 different solid carrier (sugar beads, granular sugar, maltodextrin, Avicel pH 200 and Avicel CL 611) at varying levels of film dispersing agent (additive) and danazol content as follows.

(Avicel is a trademark of FMC.)

10

TABLE 1

Run #	Additives	Ratio Of Additive to Danazol mg/gm	Grams Danazol/M ² Substrate	Substrate
1	Blg-1186-074	low	low	Sugar Beads
2	Blg-1186-063	high	high	Maltodextrin
3	Blg-1186-075	low	low	Granular Sugar
4	Blg-1186-060	high	high	Granular sugar
5	Blg-1186-069	low	high	Sugar Beads
6	Blg-1186-072	low	high	Avicel PH200
7	Blg-1186-076	low	low	Avicel PH200
8	Blg-1186-073	low	high	Avicel CL611
9	Blg-1186-061	high	high	Avicel PH200
10	Blg-1186-071	low	high	Maltodextrin
11	Blg-1186-065	high	low	Granular Sugar
12	Blg-1186-077	low	low	Avicel CL611
13	Blg-1186-066	high	low	Avicel PH200
14	Blg-1186-068	high	low	Maltodextrin
15	Blg-1186-078	low	low	Maltodextrin
16	Blg-1186-059	high	high	Sugar Beads
17	Blg-1186-067	high	low	Avicel CL611
18	Blg-1186-070	low	high	Granular Sugar
19	Blg-1186-062	high	high	Avicel CL611
20	Blg-1186-064	high	low	Sugar Beads

[0064] The beads were tested for aqueous dissolution rate using a distek 6 vessel dissolution bath at 37°C, stirring at 300 rpm using paddles. Test media was 1 liter distilled water, equilibrated to 37°C. A stainless steel sampling probe was connected to tygon tubing, and an Ismatec SA peristaltic pump was used to control flow at ~0.18 ml/min. An inline 0.020 µm filter was used to remove particulate danazol and carrier debris and to ensure that danazol detected was actually in solution. A fresh filter was used for each test vessel. An amount of formulation equivalent to 20 mg of danazol was added to the test vessel and absorbance was monitored continuously for 20 minutes at 285 nm using a Waters 990 Photodiode Array system. The Waters 990 software was then used to form a rate plot by taking the differential of the absorbance vs. time curve. The maximum point on the rate plot was noted as the maximum rate of aqueous dissolution. The two Avicel carriers used in this study were both insoluble. The Avicel PH 200 was sized at approximately 60 µm (uncoated) and retained its form as an insoluble particle during the dissolution process. Because of it's size, a 10 µm solvent filter was placed on the end of the stainless steel sampling probe preventing clogging of the probe and the 0.020 µm in-line filter.

55

[0065] The Avicel CL 611 carrier was slightly smaller in size than the Avicel PH 200 in powder form, but immediately swelled in the presence of water to a size of approximately 60 µm. During the dissolution assay, the constant agitation and 37°C temperature caused the Avicel CL 611 to break up into gelatinous particles in the 200 nm size range. All

attempts to filter these particles failed. The gelatinous form of the Avicel CL 611 quickly and consistently clogged 0.2 μm and 0.1 μm filters placed inline before the 0.02 μm filter. For this reason, no aqueous dissolution data was obtained for the Avicel CL 611 formulations.

5 Sample preparation for Aqueous Redispersion Particle Size Analysis

[0066]

- High Danazol Content Formulations: An amount of formulation equivalent to 50 mg of danazol was weighed into a 4 ml glass vial to which 1 ml of distilled water (room temperature) was added. The vial was capped and contents vortexed vigorously for 10 seconds. The prepared sample were then shaken at 300 rpm, 37°C for 10 minutes using a LabLine Shaker Incubator, after which particle sizing was performed. All samples were prepared in duplicate.
- Low Danazol Content Formulations: An amount of formulation equivalent to 50 mg of danazol was weighed into a 20 ml glass scintillation vial to which 5 ml of room temperature distilled water was added. The vial was capped and contents vortexed vigorously for 10 seconds. The prepared samples were then shaken at 300 rpm, 37°C for 10 minutes using a LabLine Shaker Incubator, after which particle sizing was performed. All samples were prepared in duplicate.
- Special note for Avicel PH 200 samples: The Avicel PH 200 carrier was removed by filtering through a 5 μm filter just prior to sizing.
- Special note for Avicel CL 611 samples: Since the Avicel CL 611 carrier itself was breaking into the nanometer size range of danazol, no usable redispersion sizing data were obtained for these formulations.
- Sizing using the Zetasizer III: Samples were diluted in filtered (0.45 μm) distilled water, and degassed before analysis. The AZ4 cell was used for all sizing procedures. Run time for size determinations was typically 120 seconds. Output from the Zetasizer III consisted of a mean particle size in nm and a 90% v/v value.
- Sizing using the Coulter N4MD: Samples were briefly vortexed then diluted 10 μl to -15 ml in filtered (0.22 μm) deionized water. Diluted samples were shaken to obtain a homogeneous suspension. A 4.5 ml cuvette was cleaned and filtered (0.22 μm) deionized water, filled half way with filtered water, and sonicated for -5 seconds to remove air bubbles. A minimal amount of the diluted sample was then added to impart a slight opaqueness to the contents of the cuvette. The cuvette was capped and inverted several times to allow proper mixing. The outside of the cuvette was siped completely dry and clean and placed into the sizing chamber which was maintained at 37°C. The viscosity setting was 0.693 cp and the refractive index was set to 1.331. The cuvette contents were adjusted as necessary to achieve a sample intensity in the range of 1.5×10^5 to 2.5×10^5 counts/second. Run time for particle sizing was typically 200 seconds. Output consisted of a mean particle size in nm, standard deviation, and a % Dust value.

40

Sugar Bead Formulations

[0067] Maximum aqueous dissolution rate values and redispersion particle sizing data are found in Table 2. The data clearly shows that the formulations containing the "high" additive ratio (Run #20 and #16) exhibited higher maximum aqueous dissolution rates and smaller particle sizes upon redispersion in water than their "low" additive ratio counterparts.

Granular Dextrose Formulations

[0068] Maximum aqueous dissolution rate values and redispersion particle sizing data are found in Table 3. On the granular matrix, there appears to be little difference in maximum aqueous dissolution rate among the 4 formulations. It can be seen, however, that the "high" additive ratio formulations (Run #11 and #4) resulted in smaller particle sizes upon redispersion compared to the two "low" additive ratio formulations.

55

Maltodextrin Formulations

[0069] Maximum aqueous dissolution rate values and redispersion particle sizing data are found in Table 4. The same pattern is observed here as in the granular dextrose formulations. The maximum aqueous dissolution rates are

all high and similar. The "high" additive ratio formulations (Run #14 and #2) exhibit smaller redispersion particle sizes than the "low" additive formulations.

Avicel PH 200 Formulations

5

[0070] Maximum aqueous dissolution rate values and redispersion particle sizing data are found in Table 5. Results from the Avicel PH 200 matrix formulations closely mimic results of those formulations on the sugar bead matrix. The "high" additive ratio formulations (Run #13 and #9) exhibited higher maximum aqueous dissolution rates compared to the formulations containing the "low" additive ratio, and their redispersion particle sizes were much smaller as well, 10 keeping with the trend observed in the previous three matrices.

Table 2

Bead Formulations							
Run #1							
Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
	5.3	3.6	299	670	371	180	17
	3.4	3.4	308	680	347	150	8
25	Mean	4.4	3.6	304	359		
	SD	1.0	0.2	6	17		
Run #5							
Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
	3.1	4.4	271	580	274	45	18
	3.6	3.8	283	620	>3 μ m		
35	Mean	3.3	4.1	277	>3 μ m		
	SD	0.3	0.3	8			
Run #20							
Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
	6.4	2.0	223	430	268	100	0
	8.4	1.8	224	455	279	50	0
50	Mean	7.8	2.1	224	274		
	SD	1.3	0.3	1	8		

55

EP 0 812 187 B1

Table 2 (continued)

Bead Formulations								
Run #16								
	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
10		8.0	2.6	213	410	240	37	6
		8.8	2.6	215	420	224	63	12
		7.4	2.8					
15	Mean	8.1	2.7	214		232		
	SD	0.7	0.1	1		11		

Table 3

Granular Dextrose Formulations								
Run #3								
	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Duet
30		7.4	2.8	241	500	262	48	9
		6.6	2.8	239	520	255	66	7
		6.0	2.6					
35	Mean	6.7	2.7	240		259		
	SD	0.7	0.1	1		5		
Run #18								
	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
40		8.4	2.8	306	700	289	36	10
		5.8	2.8	315	710	272	50	16
		6.5	3.0					
45	Mean	6.9	2.9	311		281		
	SD	1.3	0.1	6		12		
Run #11								
	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
55		6.0	2.8	210	380	229	26	0
		7.0	3.0	205	400	224	62	8
		6.7	2.8					

EP 0 812 187 B1

Table 3 (continued)

Granular Dextrose Formulations								
Run #11								
5	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
10	Mean	6.6	2.9	208		227		
	SD	0.5	0.1	4		4		
Run #4								
15	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (mm)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
20		9.0	2.8	214	390	211	29	5
		7.2	2.6	216	420	240	42	1
25	Mean	8.4	2.6	215		226		
	SD	1.0	0.2	1		21		

Table 4

Maltodextrin Formulations								
Run #15								
30	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
35		7.0	3.0	972	2200	>3 μ m		
		7.5	2.6	1282	3200	>3 μ m		
40	Mean	7.3	2.8	1127		>3 μ m		
	SD	0.3	0.2	219				
Run #10								
45	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
50		8.0	2.3	653	1150	>3 μ m		
		7.8	2.5	530	1300	>3 μ m		
55	Mean	7.6	2.5	592		>3 μ m		
	SD	0.5	0.2	87				

EP 0 812 187 B1

Table 4 (continued)

Maltodextrin Formulations								
Run #14								
5	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
10		6.9 6.5 7.4	3.0 2.8 2.7	307 326	680 720	331 286	120 35	7 5
15	Mean SD	6.9 0.5	2.8 0.2	317 13		309 32		
Run #2								
20	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
25		8.3 9.0	2.6 2.4	343 247	730 520	267 281	46 39	7 0
30	Mean SD	8.7 0.5	2.5 0.1	295 68		274 10		

Table 5

Avicel PH200 Formulations								
Run #7								
35	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
40		5.0 3.0	3.1 3.0	250 255	490 420	278 251	41 43	0 6
45	Mean SD	4.0 1.4	3.1 0.1	253 4		265 19		
Run #6								
50	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90%<Value (nm)	Coulter N4MD Size (nm)	SD	% Dust
55		3.2 2.9	3.2 3.3	254 256	525 500	254 258	44 45	5 4
55	Mean SD	3.1 0.2	3.3 0.1	255 1		256 3		

Table 5 (continued)

Avicel PH200 Formulations							
Run #13							
5	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90% < Value (nm)	Coulter N4MD Size (nm)	SD
10		6.2	3.0	214	400	219	21
		5.0	3.6	209	370	214	37
15	Mean	5.6	3.3	212		217	
	SD	0.8	0.4	4		4	
Run #9							
20	Low/Low	Maximum Aqueous Dissolution Rate ($\times 10^{-5}$ AU/min)	Time to Maximum Rate (min)	Size (nm)	90% < Value (nm)	Coulter N4MD Size (nm)	SD
		6.5	3.0	229	370	212	29
		5.7	3.3	212	420	207	32
25	Mean	6.1	3.2	221		210	
	SD	0.6	0.2	12		4	

Example 3 - Preparation of Pharmaceutical Compositions and Test for Reconstitution

30 [0071] A material having the following composition was formulated:

			% w/w
35	<u>Drug Coat:</u>		
	1.	Danazol, USP	15.1
	2.	Povidone (k15/17), USP	4.52
	3.	Sodium Lauryl Sulfate, USP	1.13
	4.	Purified Water, USP	---
40	<u>Overcoat</u>		
	5.	Povidone (k15.17), USP	0.847
	6.	Polyethylene Glycol 1000, NF	0.148
	7.	Purified Water, USP	---
45	<u>Carrier</u>		
	8.	Sugar Spheres (20-25 mesh),	NF 78.3
50	<u>Range</u>	(Drug Coat) / Danazol/Povidone Ratio 10 to 1 to 1 to 1	
	<u>Range</u>	Overcoat to Povidone 0.5 to 3.6 (w/w)	

55 [0072] The pharmaceutical composition of Example 3 was used in vitro tests in fasted male beagle dogs and compared to a commercial Danocrine formulation as to relative oral bioavailability (mean AVC under the curve (AVC) at 20mg/kg \pm Standard Error of the Mean (SEM). The oral AVC showed that the nanoparticulate Example 3 composition had a mean AVC. of 9860 ± 2600 and 11988 ± 3448 in 2 separate runs and the commercial Danocrine composition

had an AVC \pm SEM of 1076 ± 391 (20mg/kg).

[0073] This indicated that the formulation of Example 3 achieved a 10X increase in absorption over that of the standard Danocrine formulation.

5 Example 4 - Naproxen And Danazol Compositions

[0074]

	A	B
10		
	Naproxen	70.4
	Povidone	4.22
	Sucrose	21.1
15	Sodium Lauryl	4.22
	Sulfate	3.82
	Mannitol	---
		9.55
20		
		C
	Danazol	40.0
	Povidone	12.0
	Sodium Lauryl	3.0
	Sulfate	1.5
25	Dextrose	---
	Maltodextran	72.5
		45.0

[0075] The reconstituted mean particle size was found to be less than 300 nm. The procedure used to determine the ease of reconstituting particles is as follows:

- 30 1. Weigh out appropriate amount of formulation, (eg, insoluble drug equivalent to 50 mg).
2. Add 1 to 10 ml of dispersion media (distilled water, 0.1NHCl, simulated gastric or intestinal fluid, etc.)
3. Vortex the mixture for 10 seconds.
- 35 4. Shake the prepared sample at 300 RPM, 37°C for 10 minutes using a shako incubator such as a LabLine Shaker.
5. With a pipette draw off an appropriate amount of material from the preparation for particle sizing.
- 40 6. Size the resultant dispersion by using an appropriate technique such as a laser-light scattering, Franhaufa or disc centrifugation method.

[0076] It has been found that the PVP/PEG overcoat for compositions containing danazol, PVP and sodium lauryl sulfate coated on a bead, in particular, provides physical protection for the drug layer coated on the bead without inhibiting redispersion of the drug in aqueous media.

45 **Claims**

- 50 1. A solid nanoparticulate pharmaceutical composition comprising:
 - (a) a solid carrier composition, and coated onto the solid carrier composition
 - (b) a nanoparticulate drug matrix composition comprising:
 - 55 (1) a nanoparticulate crystalline drug having a solubility in water of less than 10 mg/ml;
 - (2) 0.1% to 90%, based on the weight of the drug, of a hydrophilic or amphophilic steric stabilizer associated with the surface of the nanoparticulate drug; and
 - (3) 0.05% to 50%, based on the weight of the drug, of a water-soluble film dispersing agent associated

with the surface of the drug,

wherein dissolution of the solid carrier composition results in substantial redispersion of the nanoparticulate drug particles.

- 5 2. The composition of claim 1, wherein the concentration of the steric stabilizer in the nanoparticulate drug matrix composition is 0.1% to 60%, based on the weight of the drug.
- 10 3. The composition of claim 1, wherein the drug has a solubility of less than 1 part in greater than 1,000,000 parts water.
4. The composition of claim 1, wherein the drug nanoparticles have an effective average particle size of less than 400 nm.
- 15 5. The composition according to any of the preceding claims, wherein the drug is selected from the group consisting of analgesics, anti-inflammatory agents, antihelminitics, anti-arrhythmic agents, antibiotics, anticoagulants, antidepressants, antidiabetic agents, antiepileptics, antihistamines, antihypertensive agents, antimuscarinic agents, antimycobacterial agents, antineoplastic agents, immunosuppressants, antithyroid agents, antiviral agents, anxiolytic sedatives, astringents, beta-adrenoceptor blocking agents, blood products and substitutes, cardiac inotropic agents, contrast media, corticosteroids, cough suppressants, diagnostic agents, diagnostic imaging agents, diuretics, dopaminergics, haemostatics, immunological agents, lipid regulating agents, muscle relaxants, parasympathomimetics, parathyroid calcitonin and biphosphonates, prostaglandins, radio-pharmaceuticals, sex hormones, anti-allergic agents, stimulants, anorectics, sympathomimetics, thyroid agents, vasodilators, and xanthines.
- 20 6. The composition of claim 4, wherein the drug is danazol, naproxen, or cyclosporin.
7. The composition according to any of the preceding claims, wherein the steric stabilizer is selected from the group consisting of gelatin, casein, lecithin, gum acacia, cholesterol, tragacanth, sorbitan esters, polyoxyethylene alkyl esters, polyoxyethylene caster oil derivatives, polyoxyethylene, sorbitan fatty acid esters, polyethylene glycols, 30 polyoxyethylene stearates, carboxymethylcellulose calcium, carboxymethylcellulose sodium, methylcellulose, hydroxyethylcellulose, hydroxypropylcellulose, hydroxypropylmethylcellulose, phthalate, non crystalline cellulose, polyvinyl alcohol, and polyvinylpyrrolidone.
- 35 8. The composition of claim 6, wherein the steric stabilizer is polyvinylpyrrolidone.
9. The composition of according to any of the preceding claims, wherein the film dispersing agent is selected from the group consisting of mannitol, sodium lauryl sulfate, mono saccharides, and disaccharides.
10. The composition of claim 7, wherein the film dispersing agent is sodium lauryl sulfate.
- 40 11. The composition according to any of the preceding claims, wherein the carrier particle is selected from the group consisting of sugar spheres, maltodextrin, microcrystalline cellulose, microcrystal cellulose/sodium carboxymethylcellulose, granular dextrose, granular sugar, dicalcium phosphate, tricalcium phosphate, mono saccharides, and disaccharides.
- 45 12. The composition according to claim 9, wherein the carrier particle is Avicel, lactose, granular sugar, mannitol, or dextrose.
13. The composition according to any of the preceding claims, wherein the carrier particle has a size selected from the group consisting of 40-45 mesh, 30-35 mesh, 20-25 mesh, 18-20 mesh, and 16-18 mesh.
- 50 14. The composition of claim 11, wherein the carrier particle comprises sugar spheres having from 20 to 25 mesh.
15. The composition according to any of the preceding claims, further comprising a coating of polyvinylpyrrolidone (PVP) and polyethylene glycol (PEG) over the nanoparticulate drug and film dispersing agent composition coated onto the carrier particle.
- 55 16. The composition of claim 13, wherein the polyethylene glycol has a molecular weight of from 300 to 8000.

17. The composition of claims 13 or 14, wherein the weight ratio of PEG/PVP is from 1 to 5.

18. The composition according to any of the preceding claims, wherein the composition is contained in a pharmaceutically acceptable capsule shell.

5 19. The composition of claim 16, wherein the capsule shell is a gelating capsule shell.

20. A composition as defined in any one of claims 1-19 for use as a medicament.

10

Patentansprüche

1. Feste nanopartikuläre pharmazeutische Zusammensetzung, umfassend:

15 a) eine feste Trägerzusammensetzung, und aufgetragen auf die feste Trägerzusammensetzung
b) eine nanopartikuläre Wirkstoffmatrix-Zusammensetzung, umfassend:

20 (1) einen nanopartikulären kristallinen Wirkstoff mit einer Löslichkeit in Wasser von weniger als 10 mg/ml;
(2) 0,1 % bis 90 %, bezogen auf das Gewicht des Wirkstoffs, eines hydrophilen oder amphophilen sterischen Stabilisators, der mit der Oberfläche des nanopartikulären Wirkstoffs assoziiert ist; und
(3) 0,05 % bis 50 %, bezogen auf das Gewicht des Wirkstoffs, eines wasserlöslichen filmdispersierenden Mittels, das mit der Oberfläche des Wirkstoffs verbunden ist;

25 wobei die Auflösung der festen Trägerzusammensetzung zu einer wesentlichen Redispersierung der nanopartikulären Wirkstoffpartikel führt.

2. Zusammensetzung gemäß Anspruch 1, wobei die Konzentration des sterischen Stabilisators in der nanopartikulären Wirkstoffmatrix-Zusammensetzung 0,1 % bis 60 %, bezogen auf das Gewicht des Wirkstoffs, ist.

30 3. Zusammensetzung gemäß Anspruch 1, wobei der Wirkstoff eine Löslichkeit von weniger als 1 Teil in mehr als 1.000.000 Teilen Wasser aufweist.

4. Zusammensetzung gemäß Anspruch 1, wobei die Wirkstoffnanopartikel eine effektive durchschnittliche Partikelgröße von weniger als 400 nm aufweisen.

35 5. Zusammensetzung gemäß einem der vorhergehenden Ansprüche, wobei der Wirkstoff ausgewählt ist aus der Gruppe, bestehend aus: Analgetika, entzündungshemmenden Wirkstoffen, Anthelmintika, antiarrhythmischen Wirkstoffen, Antibiotika, Antikoagulantien, Antidepressiva, antidiabetischen Wirkstoffen, Antiepileptika, Antihistaminika, blutdrucksenkenden Wirkstoffen, antimuscarinischen Wirkstoffen, antimycobakteriellen Wirkstoffen, antineoplastischen Wirkstoffen, Immunsuppressiva, antithyreoidale Wirkstoffen, antivirale Wirkstoffen, anxiolytischen Sedativa, Adstringentien, beta-Adrenorezeptor-blockierenden Wirkstoffen, Blutprodukten und Blutersatzmitteln, kardial inotropen Wirkstoffen, Kontrastmitteln, Corticosteroiden, Hustensuppressoren, diagnostischen Mitteln, diagnostischen bildgebenden Mitteln, Diuretika, Dopaminergika, Hämostatika, immunologischen Wirkstoffen, lipidregulierenden Wirkstoffen, Muskelrelaxantien, Parasympathomimetika, parathyreoidalem Calcitonin und Biphosphonaten, Prostaglandinen, Radiopharmazeutika, Sexualhormonen, anti-allergischen Wirkstoffen, Stimulatien, Anorektika, Sympathomimetika, thyreoidalen Wirkstoffen, Vasodilatanzien und Xanthinen.

45 6. Zusammensetzung gemäß Anspruch 4, wobei der Wirkstoff Danazol, Naproxen oder Cyclosporin ist.

50 7. Zusammensetzung gemäß einem der vorhergehenden Ansprüche, wobei der sterische Stabilisator ausgewählt ist aus der Gruppe, bestehend aus: Gelatine, Casein, Lecithin, Akaziengummi, Cholesterin, Tragant, Sorbitanestern, Polyoxyethylenalkylestern, Polyoxyethylen-Ricinusöl-Derivaten, Polyoxyethylen, Sorbitanfettsäureestern, Polyethylenglycolen, Polyoxyethylenstearaten, Carboxymethylcellulose-Calcium, Carboxymethylcellulose-Natrium, Methylcellulose, Hydroxyethylcellulose, Hydroxypropylcellulose, Hydroxypropylmethylcellulose, Phthalat, nichtkristalliner Cellulose, Polyvinylalkohol und Polyvinylpyrrolidon.

55 8. Zusammensetzung gemäß Anspruch 6, wobei der sterische Stabilisator Polyvinylpyrrolidon ist.

9. Zusammensetzung gemäß einem der vorhergehenden Ansprüche, wobei das filmdispersierende Mittel ausgewählt ist aus der Gruppe, bestehend aus: Mannit, Natriumlaurylsulfat, Monosacchariden und Disacchariden.
10. Zusammensetzung gemäß Anspruch 7, wobei das filmdispersierende Mittel Natriumlaurylsulfat ist.
- 5 11. Zusammensetzung gemäß einem der vorhergehenden Ansprüche, wobei der Trägerpartikel ausgewählt ist aus der Gruppe, bestehend aus: Zuckerkugeln, Maltodextrin, mikrokristalliner Cellulose, mikrokristalliner Cellulose/Carboxymethylcellulose-Natrium, kömiger Dextrose, kömigem Zucker, Dicalciumphosphat, Tricalciumphosphat, Monosacchariden und Disacchariden.
- 10 12. Zusammensetzung gemäß Anspruch 9, wobei der Trägerpartikel Avicel, Lactose, körniger Zucker, Mannitol oder Dextrose ist.
- 15 13. Zusammensetzung gemäß einem der vorhergehenden Ansprüche, wobei der Trägerpartikel eine Größe aufweist, die ausgewählt ist aus der Gruppe, bestehend aus: 40-45 mesh, 30-35 mesh, 20-25 mesh, 18-20 mesh und 16-18 mesh.
14. Zusammensetzung gemäß Anspruch 11, wobei der Trägerpartikel Zuckerkugeln von 20 bis 25 mesh umfasst.
- 20 15. Zusammensetzung gemäß einem der vorhergehenden Ansprüche, weiter umfassend einen Überzug aus Polyvinylpyrrolidon (PVP) und Polyethylenglycol (PEG) über der Zusammensetzung aus dem nanopartikulären Wirkstoff und dem filmdispersierenden Mittel, die auf dem Trägerpartikel aufgetragen ist.
16. Zusammensetzung gemäß Anspruch 13, wobei das Polyethylenglycol ein Molekulargewicht von 300 bis 8000 aufweist.
- 25 17. Zusammensetzung gemäß einem der Ansprüche 13 oder 14, wobei das Gewichtsverhältnis PEG/PVP 1 bis 5 beträgt.
18. Zusammensetzung gemäß einem der vorhergehenden Ansprüche, wobei die Zusammensetzung in einer pharmazeutisch verträglichen Kapselhülle enthalten ist.
- 30 19. Zusammensetzung gemäß Anspruch 16, wobei die Kapselhülle eine gelatinierende Kapselhülle ist.
20. Zusammensetzung wie in einem der Ansprüche 1-19 definiert zur Verwendung als Arzneimittel.

Revendications

- 40 1. Composition pharmaceutique solide de nanoparticules, comprenant :
 - (a) une composition solide de support et, appliquée sous forme d'un revêtement sur la composition solide de support
 - (b) une composition de matrice médicamenteuse en nanoparticules comprenant :
 - (1) un médicament cristallin en nanoparticules ayant une solubilité dans l'eau inférieure à 10 mg/ml ;
 - (2) 0,1 % à 90 %, sur la base du poids du médicament, d'un stabilisant stérique hydrophile ou amphophile associé à la surface du médicament en nanoparticules ; et
 - (3) 0,05 % à 50 %, sur la base du poids du médicament, d'un agent hydrosoluble de dispersion de film associé à la surface du médicament ;
- 45 dans laquelle la dissolution de la composition solide de support a pour résultat une redispersion substantielle des particules du médicament en nanoparticules.
- 50 2. Composition suivant la revendication 1, dans laquelle la concentration du stabilisant stérique dans la composition de matrice de médicament en nanoparticules est de 0,1 % à 60 %, sur la base du poids du médicament.
3. Composition suivant la revendication 1, dans laquelle le médicament a une solubilité inférieure à 1 partie dans

plus de 1 000 000 parties d'eau.

4. Composition suivant la revendication 1, dans laquelle les nanoparticules de médicament ont une dimension particulière moyenne effective de inférieur à 400 nm.
5. Composition suivant l'une quelconque des revendications précédentes, dans laquelle le médicament est choisi dans le groupe consistant en des analgésiques, des agents anti-inflammatoires, des antihelminthiques, des agents anti-arythmiques, des antibiotiques, des anticoagulants, des antidépresseurs, des agents antidiabétiques, des anti-épileptiques, des anti-histaminiques, des agents anti-hypertenseurs, des agents antimuscariniques, des agents antimycobactériens, des agents antinéoplasiques, des immuno-supresseurs, des agents antithyroïdiens, des agents antiviraux, des sédatifs anxiolytiques, des astringents, des agents de blocage des bêta-adrénorécepteurs, des produits sanguins et produits de substitution du sang, des agents inotropes cardiaques, des milieux de contraste, des corticostéroïdes, des antitussifs, des agents de diagnostic, des agents d'imagerie de diagnostic, des diurétiques, des dopamnergiques, des hémostatiques, des agents immunologiques, des agents de régulation des lipides, des myorelaxants, des parasympathomimétiques, la calcitonine parathyroïdiennes et des biphosphonates, des prostaglandines, des agents radio-pharmaceutiques, des hormones sexuelles, des agents anti-allergiques, des stimulants, des anorexi-gènes, des sympathomimétiques, des agents thyroïdiens, des vasodilatateurs et des xanthines.
6. Composition suivant la revendication 4, dans laquelle le médicament est le danazol, le naproxène ou la cyclosporine.
7. Composition suivant l'une quelconque des revendications précédentes, dans laquelle le stabilisant stérique est choisi dans le groupe consistant en la gélatine, la caséine, la lécithine, la gomme d'acacia, le cholestérol, la gomme adragante, les esters de sorbitane, des esters alkyliques de polyoxyéthylène, des dérivés d'huile de ricin et de polyoxyéthylène, la polyoxyéthylène, des esters d'acides gras de sorbitane et de polyoxyéthylène, des polyéthylène-glycols, des stéarates de polyoxyéthylène, la carboxyméthylcellulose calcique, la carboxyméthylcellulose sodique, la méthylcellulose, l'hydroxyéthylcellulose, l'hydroxypropylcellulose, l'hydroxypropylméthylcellulose, des phtalates, la cellulose non cristalline, l'alcool polyvinyle et la polyvinylpyrrolidone.
8. Composition suivant la revendication 6, dans laquelle le stabilisant stérique est la polyvinyl-pyrrolidone.
9. Composition suivant l'une quelconque des revendications précédentes, dans laquelle l'agent de dispersion de film est choisi parmi le groupe consistant en le mannitol, le laurylsulfate de sodium, les mono-saccharides et les disaccharides.
10. Composition suivant la revendication 7, dans laquelle l'agent de dispersion de film est le laurylsulfate de sodium
11. Composition suivant l'une quelconque des revendications précédentes, dans laquelle la particule de support est choisie dans le groupe consistant en des sphères de sucre, la maltodextrine, la cellulose microcristalline, la cellulose microcristalline/carboxy-méthylcellulose sodique, le dextrose granulaire, le sucre granulaire, le phosphate dicalcique, le phosphate tricalcique, des monosaccharides et des disaccharides.
12. Composition suivant la revendication 9, dans laquelle la particule de support est constituée d'Avicel, de lactose, de sucre granulaire, de mannitol ou de dextrose.
13. Composition suivant l'une quelconque des revendications précédentes, dans laquelle la particule de support a une dimension choisi dans le groupe consistant en de 40 à 45 mesh, de 30 à 35 mesh, de 20 à 25 mesh, de 18 à 20 mesh et de 16 à 18 mesh.
14. Composition suivant la revendication 11, dans laquelle la particule de support comprend des sphères de sucre ayant une dimension de 20 à 25 mesh.
15. Composition suivant l'une quelconque des revendications précédentes, comprenant en outre un revêtement de polyvinylpyrrolidone (PVP) et de polyéthylèneglycol (PEG) sur le médicament en nanoparticules et la composition d'agent de dispersion de film présente sous forme d'un revêtement sur la particule de support.
16. Composition suivant la revendication 13, dans laquelle le polyéthylèneglycol a un poids moléculaire de 300 à 8000.

17. Composition suivant la revendication 13 ou 14, dans laquelle le rapport pondéral PEG/PVP est un rapport de 1 à 5.
18. Composition suivant l'une quelconque des revendications précédentes, qui est présente dans une enveloppe de capsule pharmaceutiquement acceptable.
- 5 19. Composition suivant la revendication 16, dans laquelle l'enveloppe de capsule est une enveloppe de capsule en gélatine.
- 10 20. Composition répondant à la définition suivant l'une quelconque des revendications 1 à 19, destinée à être utilisée comme médicament.

15

20

25

30

35

40

45

50

55